How intelligent is artificial intelligence? – On the surprising and mysterious secrets of deep learning

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Computers can be made to see a sea turtle as a gun or hear a concerto as someone's voice, which is raising concerns about using artificial intelligence in the real world. What could possibly go wrong?

Al replacing standard algorithms

Mathematical setup

Image reconstruction in medical imaging

- ▶ $x \in \mathbb{C}^N$ the true image (interpreted as a vector).
- ▶ $A \in \mathbb{C}^{m \times N}$ measurement matrix (m < N).
- \triangleright y = Ax the measurements.

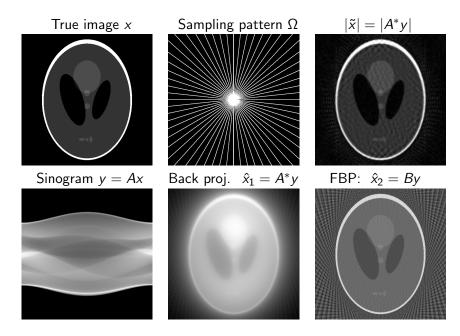


Image reconstruction methods

▶ Deep learning approach: For a given a set $\{x_1, \dots, x_n\}$, train a neural network $f: \mathbb{C}^m \to \mathbb{C}^N$ such that

$$||f(Ax_i) - x_i|| \ll ||A^*x_i - x_i||$$

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► Sparse regularization

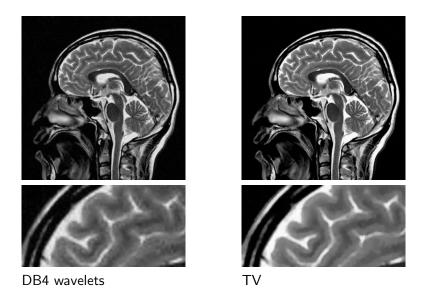
$$\text{minimize}_{z \in \mathbb{C}^N} \, \| \, \textit{Wz} \|_{\ell_1} \quad \text{subject to} \quad \| \textit{Az} - \textit{y} \|_{\ell_2} \leq \eta$$

Image x





Sparse regularization reconstruction



Typical sparse regularization result

Let $A \in \mathbb{C}^{m \times N}$ with m < N and y = Ax + e, with $\|e\|_2 \le \eta$. Let $W \in \mathbb{C}^{N \times N}$ be unitary, and suppose that AW^{-1} satisfies the restricted isometry property in levels (RIPL). Then any minimizer \hat{x} of

$$\operatorname{minimize}_{z \in \mathbb{C}^N} \| \mathit{Wz} \|_1 \quad \text{subject to} \quad \| \mathit{Az} - y \| \leq \eta$$

satisfies

$$||\hat{x} - x||_2 \lesssim \frac{\sigma_{\mathsf{s},\mathsf{M}}(\mathit{W}x)_1}{\sqrt{s}} + \eta$$

where

$$\sigma_{\mathbf{s},\mathbf{M}}(Wx)_1 = \inf\{||Wx - z||_1 : z \text{ is } (\mathbf{s},\mathbf{M})\text{-sparse}\}$$

Pure denoisers. Train a neural network ϕ to learn the noise.

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- ▶ Data consistent denoisers. Train n networks ϕ_i , i = 1, ..., n and ensure that the final image is consistent with your data
 - 1: Pick $\alpha \in [0, 1]$.
 - 2: Set $\tilde{y}_1 = y$.
 - 3: **for** i = 1, ... n **do**
 - 4: $\tilde{\mathbf{x}}_i = \mathbf{A}^* \tilde{\mathbf{y}}_i \phi_i (\mathbf{A}^* \tilde{\mathbf{y}}_i)$
 - 5: $\hat{y} = A\tilde{x}_i$
 - 6: $\tilde{y}_{i+1} = \alpha \hat{y} + (1 \alpha)y$, (Enforce data consistency)
 - 7: **Return:** \tilde{x}_n .

Learn the physics. Do **not** warm start your network with A^* .

Rather learn
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- ▶ Unravel n steps with sparse regularization solver. Learn λ_i , K_i , and Ψ_i for i = 1, ..., n.
 - 1: $x_1 = A^* y$
 - 2: **for** i = 1, ... n **do**
 - 3: $\tilde{x}_{i+1} = \tilde{x}_i (K_i)^T \Psi_i(K_i \tilde{x}_i) + \lambda_i A^* (A \tilde{x}_i y)$
 - 4: **Return:** \tilde{x}_{n+1} .

(omitting some details here)

Networks considered

► AUTOMAP

- ► Low resolution images, 60% subsampling, single coil MRI.
- B. Zhu, J. Z. Liu, S. F. Cauley, B. R. Rosen and M. S. Rosen, 'Image reconstruction by domain-transform manifold learning', Nature, vol. 555, no. 7697, p. 487, Mar. 2018.

DAGAN

- Medium resolution, 20% subsampling, single coil MRI.
- G. Yang, S. Yu, H. Dong, G. Slabaugh, P. L. Dragotti, X. Ye, F. Liu, S. Arridge, J. Keegan, Y. Guo et al., DAGAN: Deep de-aliasing generative adversarial networks for fast compressed sensing MRI reconstruction, IEEE Transactions on Medical Imaging, 2017.

Deep MRI

- Medium resolution, 33% subsampling, single coil MRI.
- J. Schlemper, J. Caballero, J. V. Hajnal, A. Price and D. Rueckert, A deep cascade of convolutional neural networks for MR image reconstruction, in International conference on information processing in medical imaging, Springer, 2017, pp. 647–658.

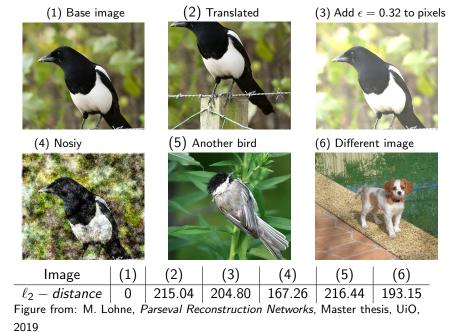
Networks considered

- ► Ell 50 and Med 50 (FBPConvNet)
 - ► CT or any Radon transform based inverse problem, with 50 uniformly spaced lines.
 - K. H. Jin, M. T. McCann, E. Froustey and M. Unser, 'Deep convolutional neural network for inverse problems in imaging', IEEE Transactions on Image Processing, vol. 26, no. 9, pp. 4509–4522, 2017.

MRI-VN

- Medium to high resolution, parallel MRI with 15 coil elements and 15% subsampling.
- K. Hammernik, T. Klatzer, E. Kobler, M. P. Recht, D. K. Sodickson, T. Pock and F. Knoll, 'Learning a variational network for reconstruction of accelerated MRI data', Magnetic resonance in medicine, vol. 79, no. 6, pp. 3055–3071, 2018.

How to measure image quality?



Three types of instabilities

- (1) Instabilities with respect to tiny perturbations. That is $\tilde{y} = A(x+r)$ with ||r|| very small.
- (2) Instabilities with respect to small structural changes, for example a tumour, may not be captured in the reconstructed image
- (3) Instabilities with respect to changes in the number of samples. Having more information should increase performance.

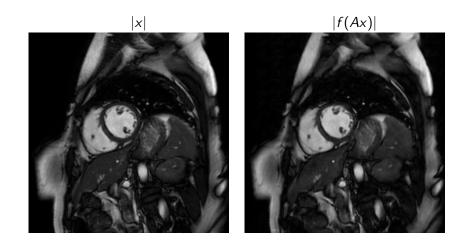
V. Antun, F. Renna, C. Poon, B.Adcock, A. Hansen. *On instabilities of deep learning in image reconstruction - Does AI come at a cost?* (arXiv 2019)

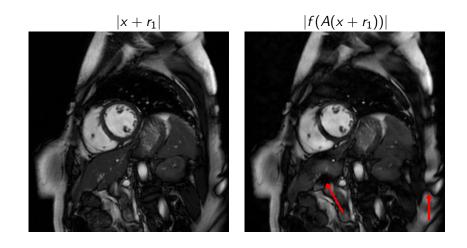
Finding tiny perturbations

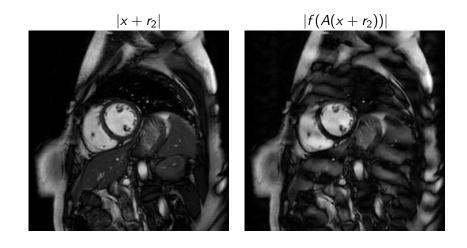
Try to maximize

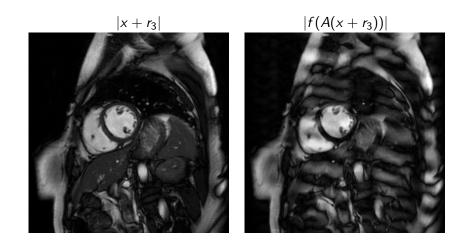
$$Q_{x}(r) = \frac{1}{2} \|f(A(x+r)) - f(Ax)\|_{\ell_{2}}^{2} - \frac{\lambda}{2} \|r\|_{\ell_{2}}^{2}, \quad \lambda > 0$$

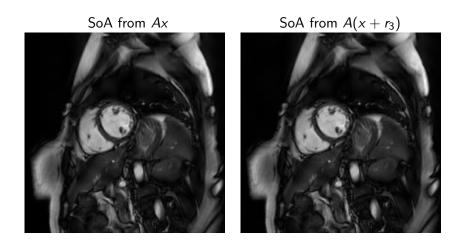
using a gradient ascent proceedure.

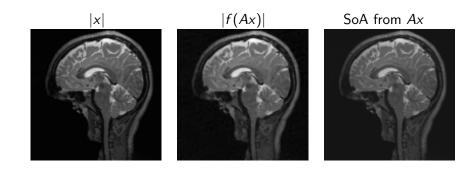


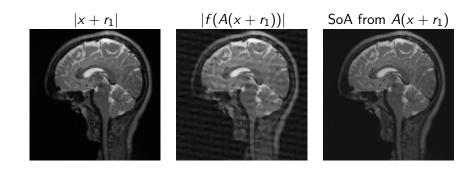


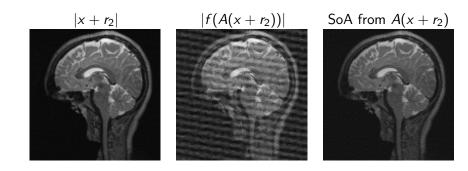


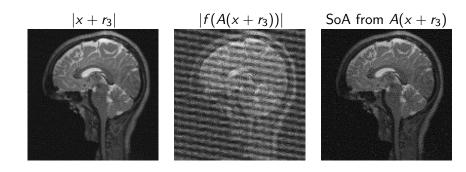


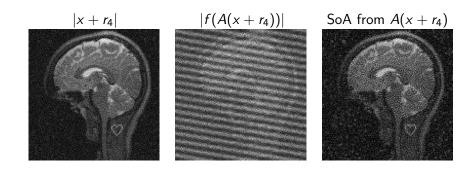










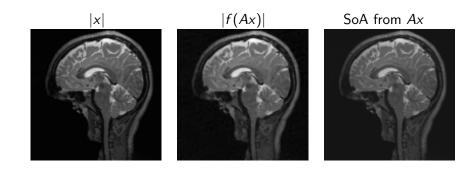


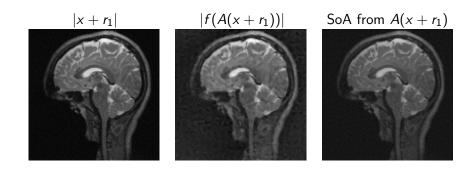
Finding tiny perturbations

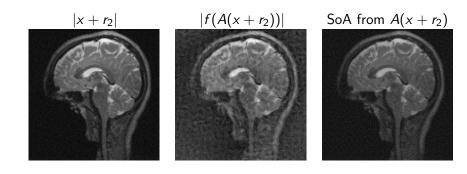
What if we tried to maximize

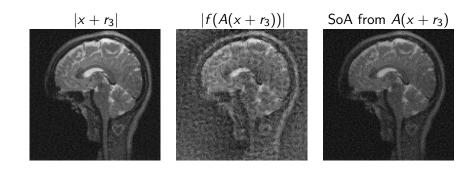
$$Q_{x}(r) = \frac{1}{2} \| f(A(x+r)) - x \|_{\ell_{2}}^{2} - \frac{\lambda}{2} \| r \|_{\ell_{2}}^{2}, \quad \lambda > 0$$

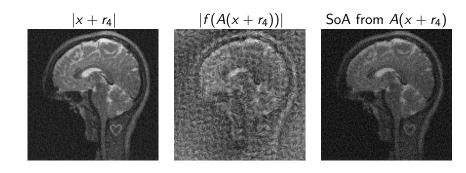
instead



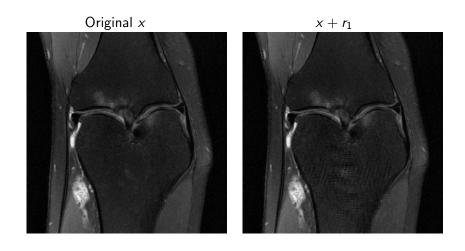




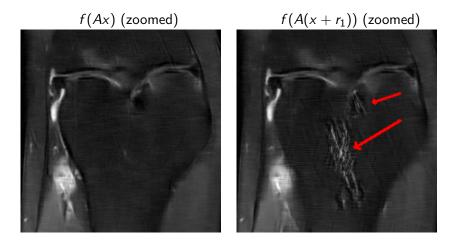




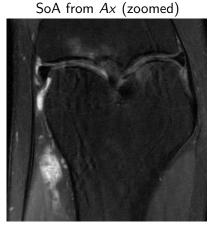
Tiny perturbation – MRI-VN

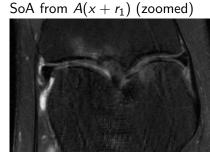


Tiny perturbation – MRI-VN

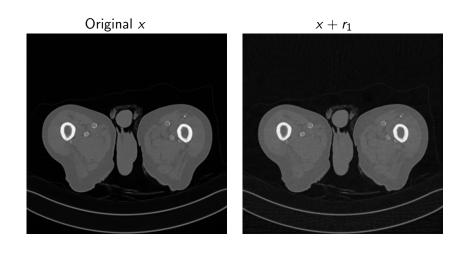


Tiny perturbation – MRI-VN

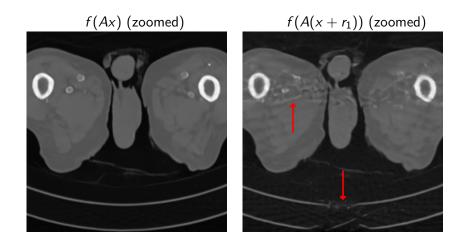




Tiny perturbation – Med 50



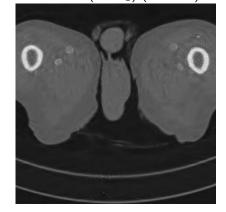
Tiny perturbation – Med 50



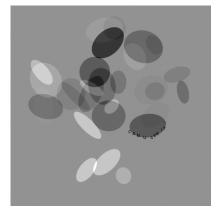
Tiny perturbation – Med 50

SoA from Ax (zoomed)

SoA from $A(x + r_1)$ (zoomed)

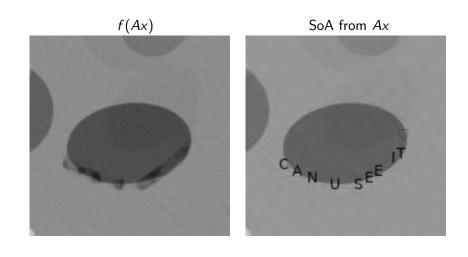


Small structural change - Ell 50

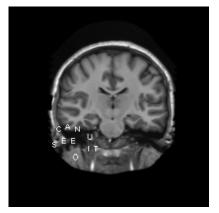


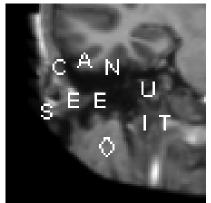


Small structural change – Ell 50

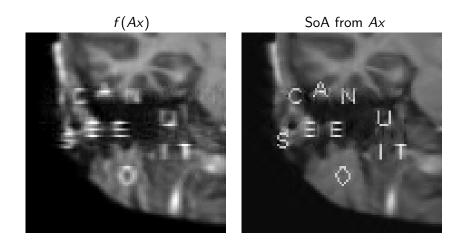


Small structural change – DAGAN

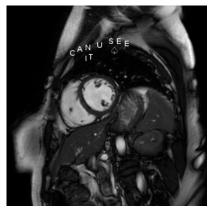




Small structural change – DAGAN

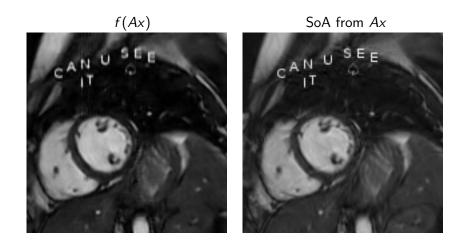


Small structural change – Deep MRI

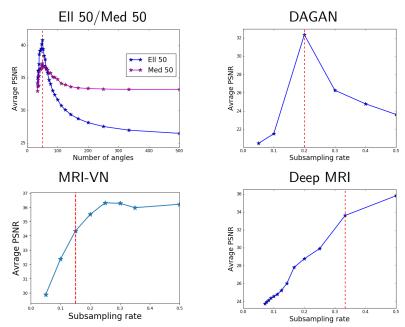




Small structural change – Deep MRI



Adding more samples

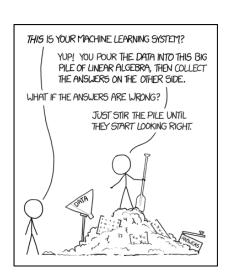


Summary of so far...

- Tiny perturbations lead to a myriad of different artefacts.
- Variety in failure of recovering structural changes.
- Networks must be retrained on any subsampling pattern?
- Universality Instabilities regardless of architecture?
- ▶ Rare events? Empirical tests are needed.

Can we fix it?

- Computational power is increasing. We can train, test and at a substantial higher rate than just a few years ago.
- ▶ The datasets are growing.
- Increased knowledge about good learning techniques



WINNER'S CURSE?

ON PACE, PROGRESS, AND EMPIRICAL RIGOR

D. Sculley, Jasper Snoek, Ali Rahimi, Alex Wiltschko

 $\{ \texttt{dsculley, jsnoek, arahimi, alexbw} \} \\ \texttt{@google.com} \\ \\ \textbf{Google AI}$

ABSTRACT

The field of ML is distinguished both by rapid innovation and rapid dissemination of results. While the pace of progress has been extraordinary by any measure, in this paper we explore potential issues that we believe to be arising as a result. In particular, we observe that the rate of empirical advancement may not have been

Troubling Trends in Machine Learning Scholarship

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July 27, 2018

1 Introduction

Collectively, machine learning (ML) researchers are engaged in the creation and dissemination of knowledge about data-driven algorithms. In a given paper, researchers might aspire to any subset of the following goals, among others: to theoretically characterize what is learnable, to obtain

Theorem 1

Let $A: \mathbb{C}^N \to \mathbb{C}^m$ be a linear sampling map and let $f: \mathbb{C}^m \to \mathbb{C}^N$. Suppose that there are $x, \eta, \xi_{\eta}, \xi_{x} \in \mathbb{C}^N$ with $\|\xi_{\eta}\|, \|\xi_{x}\| \leq \delta \in (0, 1/2)$ such that

$$f(Ax) = x + \xi_x, \quad f(A(x+\eta)) = x + \eta + \xi_\eta, \tag{1}$$

where $\|\eta\| = 1$ and $\|A\eta\| = \delta > 0$. Then we have the following.

(i) (Instabilities) Then the local Lipschitz constant of f at Ax, defined for $\epsilon > \delta > 0$, satisfies

$$L_{Ax}^{\epsilon} = \sup_{0 < \|Az\| \le \epsilon} \frac{\|f(Ax + Az) - f(Ax)\|}{\|Az\|}$$
$$\ge \frac{1 - 2\delta}{\epsilon}$$

Theorem 2

Let $A: \mathbb{C}^N \to \mathbb{C}^m$ be a linear sampling map and let $f: \mathbb{C}^m \to \mathbb{C}^N$. Suppose that there are $x, \eta, \xi_{\eta}, \xi_{x} \in \mathbb{C}^N$ with $\|\xi_{\eta}\|, \|\xi_{x}\| \le \delta \in (0, 1/2)$ such that

$$f(Ax) = x + \xi_x, \quad f(A(x+\eta)) = x + \eta + \xi_\eta, \tag{2}$$

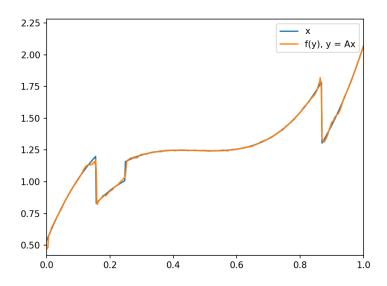
where $\|\eta\| = 1$ and $\|A\eta\| = \delta > 0$. Then we have the following.

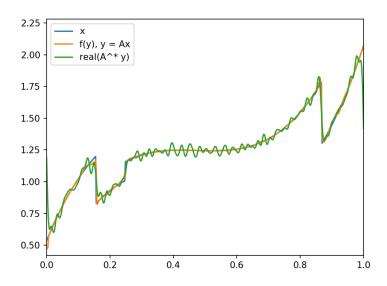
(ii) (False positives) Moreover, there exists a perturbation $r \in \mathbb{C}^m$ with $||r|| = \delta$ such that

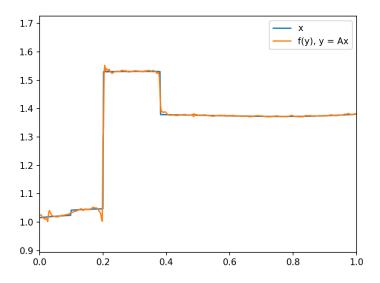
$$||f(r+Ax)-(x+\eta)||\leq \delta.$$

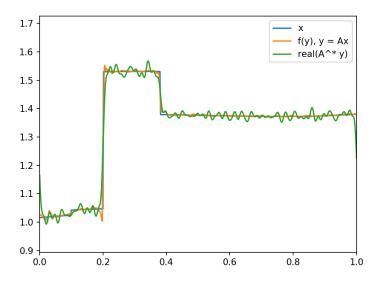
(iii) (False negatives) and there exists a perturbation $r \in \mathbb{C}^m$ with $||r|| = \delta$ such that

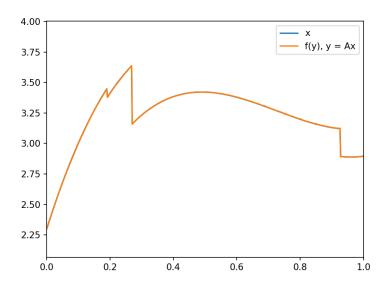
$$||f(r+A(x+\eta))-x|| \leq \delta.$$

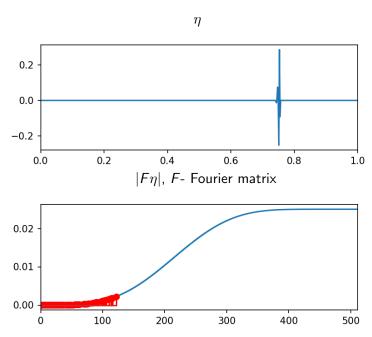


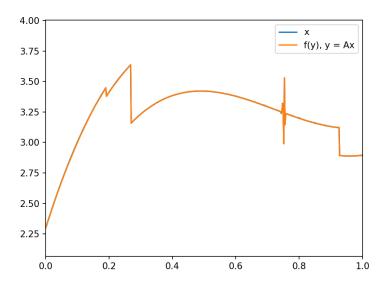


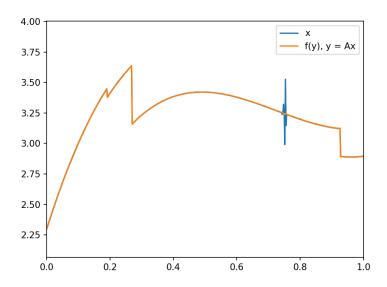


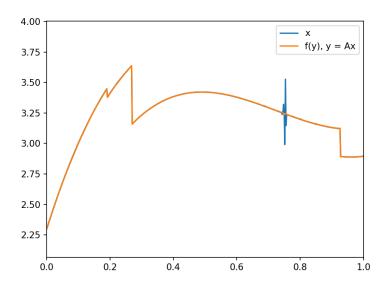


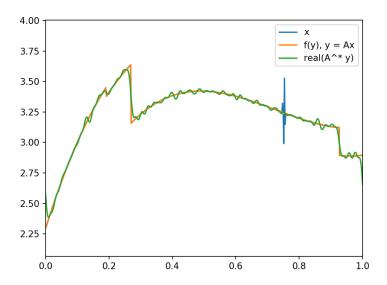


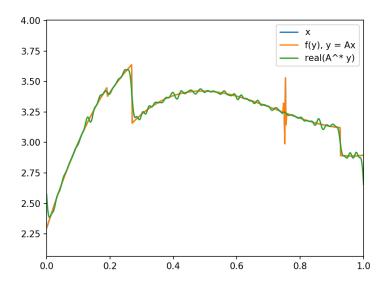












Typical sparse regularization result

Recall that if AW^{-1} satisfies the restricted isometry property in levels (RIPL).

$$\hat{x} \in \operatorname{argmin}_{z \in \mathbb{C}^N} \|Wz\|_1$$
 subject to $\|Az - y\| \le \eta$

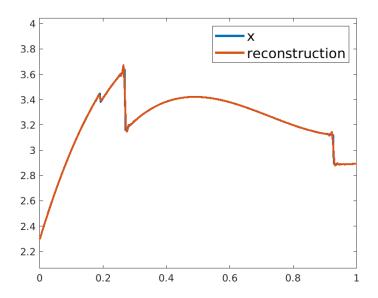
satisfies

$$||\hat{x} - x||_2 \lesssim \frac{\sigma_{\mathsf{s},\mathsf{M}}(\mathit{W}x)_1}{\sqrt{\mathsf{s}}} + \eta$$

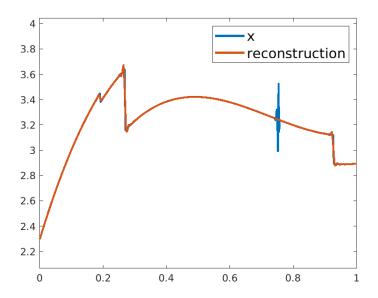
where

$$\sigma_{\mathbf{s},\mathbf{M}}(Wx)_1 = \inf\{||Wx - z||_1 : z \text{ is } (\mathbf{s},\mathbf{M})\text{-sparse}\}$$

Wavelet reconstruction



Wavelet reconstruction



Summary

Kernel awareness is important

▶ It seems hard to protect against to high preformance.

Universality – Instabilities regardless of architecture